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Influences of cell-penetrating peptide concentration on the penetration of phospholipid membrane

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Abstract. It is necessary to fully understand the interaction between the cell penetration peptide and the different types of phospholipid membranes. In this research the interaction between R9 antibacterial peptide and asymmetric phospholipid is studied by using the method of coarse-grained dynamic simulation. The investigation shows that when there is only one R9 antibacterial peptide in the system, it is hard to penetrate through the phospholipid membrane spontaneously. When the concentration of the antibacterial peptide reaches a certain value, with the help of the enhanced electrostatic interactions and the cooperative effect, the peptides will pass through the phospholipid bilayer and reach the inside of the cell. Increasing the concentration of antimicrobial peptides is helpful to improve the penetration rate of the peptides. Our results can provide some theoretical guidance for drug delivery in the biological system.

1. Introduction

Cell-penetrating peptides (CPPs), because of their ability to cross cellular membranes alone or with cargo and deliver bioactive molecules efficiently, have recently gained increasing attention from both the theoretical and experimental researchers [1-3]. As the short sequences of amino acids being usually highly cationic and hydrophilic, they can penetrate membrane more efficiently than others such as trans-activator of transcription (TAT) peptide and polylysine [4]. Since the ability of arginine-rich peptides to facilitate bioactive molecules going into cells makes them promising candidates for drug delivery, it is necessary to investigate the translocation mechanism of polyarginine peptides. During these years, many works related to peptide translocation have been done theoretically or experimentally. For instance, studies have reported that cells can internalize arginine-rich peptides by macropinocytic uptake [5]. Some experimental results indicate that the addition of penetration to brain lipids can induce inverted micelles formation [6]. Although many different classes of CPPs have been studied, the underlying mechanism with which arginine-rich peptides penetrate the cell membranes is still not understood. Thus, the exact pathway through which CPPs enter cells remains incompletely understood.

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Apart from the properties of the CPPs, membrane properties may also play an important role in the translocation. Some previous studies have considered the biomembranes as symmetric [7], however most eukaryotic cell membranes are asymmetric. For example, human erythrocyte membrane comprises phosphatidyl- choline, sphingomyelin, and glycolipids in the outer leaflet, and phosphatidylethanolamine, phosphatidylserine, and phosphatidyl- inositol in the inner leaflet [8,9]. Such asymmetry of membrane can affect biological behaviors, such as recognition by macrophages [10] and cellular uptake [11]. Therefore, we think that it is very important to further study the CPPs' translocation across asymmetric lipid bilayer. Because of the higher translocation efficiency than other CPPs, polyarginine peptides (R9) are always the focuses of many investigations. Li et al. [12] have shown that multiple polyarginine peptides can penetrate asymmetric membranes cooperatively and translocate across membranes while carrying conjugated nanoparticles (NPs). To explore the interactions between NPs and biomembranes, the coarse-grained molecular dynamics (CGMD) simulations have recently become a powerful and indispensable tool [13-15]. In the present study, we will use the CGMD simulations to investigate the effects of R9 peptide concentrations and membrane asymmetric level on the translocation mechanism. Our study may provide insights into the mechanism of interactions between peptides and asymmetric membranes at molecular level, which can impact targeted gene and drug delivery.

2. Model and Methods

CGMD simulations are used to investigate the interactions between CPPs and biomembrane because they present larger spatial and temporal scales comparing with all-atom molecular dynamics simulations [16,17]. In this paper, we will use the Martini coarse graining (CG) force field [18] to study the translocation process of the polyarginines. This force field defines four particle types, i.e., polar(P), nonpolar(N), apolar(C), and charged (Q). Within a main type, subtypes are either distinguished by one or two letters denoting the hydrogenbonding capabilities, i.e., d(donor), a (acceptor), da(both), o(none), or by a number indicating the degree of polarity (from 1, low polarity, to 5, high polarity). It should be stated that because of the smoothed energy barrier in the Martini CG force field, the effective time that the system has experienced is 4 times longer than the simulation sampling time [4], thus in this work the effective time is used to perform the simulation.

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To investigate the mechanism of peptides and membrane interactions, it is necessary to have information about the atomistic structure of peptides used. Firstly, the atomistic R9 is downloaded from the site: http://crdd.osdd.net/raghava/cppsite/ [19]. Then, the atomistic structure is converted into the coarse grained mode by using the script martinize.py downloaded from http://md. chem.rug.nl/index.php/tools2/proteins-and-bilayer following the extended Martini force field for proteins (Martini_v2.2) [20]. The CG structure is simulated 100 ns in aqueous solution. Each arginine includes three beads: the backbone bead (P5) and side chain beads (No and Qd) (Figure 2.1). Since the Qd bead bears one positive charge, the whole R9 carries a charge of +9. The bonded interaction parameters for polyarginine peptides are those as bond, angle and dihedral potential energy functions, while nonbonded interactions are represented by the L-J potential and Coulombic energy functions. Takechi et al. [21] have shown that the random coil structure of the short-chain polyarginines remain unchanged when 69 arginines interact with an anionic phospholipid large unilamellar vesicle. We do not consider the change of its helix property during the simulations, because R9 is also a shortchain peptide.

To explore the interactions of membrane and peptides in real human body, in this study an asymmetric human erythrocyte membrane model [8] is used, which includes three lipid types: dipalmitoyl phosphatidylcholine (DPPC), dipalmitoyl phosphatidy-lethanolamine (DPPE), and dipalmitoyl phosphatidylserine (DPPS). Mapping of lipid molecules based on the Martini CG force field (Martini_v2.2) [22] is shown in Figure 2.2. The lipid choline groups are coarse-

Table 2-1. Detailed description of the lipid model in the Martini CG force field.

Interaction	Туре	Equation	Parameter
Nonbonded interaction	L-J potential	$U_{LJ}(r) = 4\varepsilon_{ij} \left[\left(\frac{\sigma_{ij}}{r}\right)^{12} - \left(\frac{\sigma_{ij}}{r}\right)^{6} \right]$	$\sigma_{ij} = 0.47 nm$
	Coulombic energy	$U_{el}(r) = \frac{q_{i}q_{j}}{4\pi\varepsilon_{0}\varepsilon_{r}r}$	$\mathcal{E}_r = 15$
Bonded interaction	Bond potential energy	$V_b = \frac{1}{2} K_b (d_{ij} - d_b)^2$	$K_{\text{bond}} = 1250 \text{ KJ mol}^{-1} \text{nm}^{-2}$ $K_{\text{bond}} = 0.47 nm$
	Angle potential energy	$V_a = \frac{1}{2} K_a \Big[\cos(\theta_{ijk}) - \cos(\theta_a) \Big]^2$	K_{angle} =25 KJ mol ⁻¹ rad ⁻² $\theta_0 = 180^{\circ}$
	Dihedral angle energy	$V_{d} = K_{d} \left[1 + \cos(n\varphi_{ijkl} - \varphi_{d}) \right]$	
-0		NH	P5 No

Figure 2.1: Mapping of R9 peptide in the framework of the Martini force field.

NH2

grained to the beads Qo, Qd and P5 for DPPC, DPPE and DPPS, respectively. The phosphate groups, glycerol groups and carbon tails of all lipids are represented by Qa, Na and C1, respectively. The expressions and parameters of bonded interactions and nonbonded interactions for lipid in the Martini CG force field are shown in Table 2-1. In the outer leaflet of the membrane, the lipid ratio is 9:1 for DPPC and DPPE, while in the inner membrane leaflet, the lipid ratio is 3:5:2 for DPPC, DPPE, and DPPS, which is similar to the human erythrocyte membrane.



Figure 2.2: a) Mapping of lipid molecules in the framework of the Martini force field. b) Detailed information of the simulation box (red, green and yellow represent DPPC DPPE DPPS, respectively.)

Table 2-2.	Simulation	system
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System	Membrane	Peptides	lons	Interaction
	charge	charge		mechanism
				(penetration
				amount)
N1	51-	9+	42Na+	Adsorption
N3	51-	27+	24Na+	Adsorption
N5	51-	45+	6Na+	Penetration(1)
N7	51-	63+	12Cl-	Penetration(2)

A cuboid simulation box (only for membrane) with dimensions of $12.5 \times 12.5 \times 18 \text{ nm}^3$ is created by using the tool insane.py for each simulation system [23] which consists of 510 lipid molecules and approximately 11000 water beads, including 1000 of "antifreeze" (WF) particles to prevent spurious freezing of the Martini solvent at low temperature. The lipid number is similar to the previous studies which are 512 [24]. Sodium ions are added to maintain the neutrality of the systems, the details of which are shown in Table 2-2. Then, the 200 ns NPT equilibration is carried out to relax the system, [11] and the time step is set to 20 fs. The temperature is controlled to 323 K via the V-rescale thermostat with a relaxation time of 0.1 ps. A pressure of 1 bar is maintained with Parrinello-Rahman thermostat and the time constant is 12 ps. A cutoff distance of 1.2 nm is used for van der Waals (vdW) interactions. For electrostatic interactions, the Particle Mesh Ewald (PME) method is employed [25]. The dielectric constant is set to 15 to compensate for the neglect of explicit polarization of the Martini water model [4]. After that, we use the membrane simulated above and rebuild the system by adding the R9 peptides. Detailed information of the system box is provided in Figure 2.2. In the initial state, the center of mass distance in the z-direction between R9 and the membrane (z-distance) is 4 nm. The height of the simulation box is fixed as 18 nm in the z-direction. The systems are first minimized by using the steepest-descent method. Then, a 200 ns NPT equilibration with a force constant 1000 KJ mol⁻¹ nm⁻²

JH.